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Introduction



Hearing Loss (HL)

Approx. 35-out-of-10,000 children suffer and 33% of adults (<u>></u> 65 yrs.) are impacted by hearing loss^{1,2}

Hearing Aids (HA)

Microphone-speaker based behind-the-ear (BTE) system to amplify incoming sounds

Cochlear Implants (CI)

- Medical device used to generate electrical stimulation from an acoustic input
 - Implanted intra-cochlear electrode array
 - BTE sound processor (and mic)



HA Signal Processing



Figure 1. Example signal processing pipeline for HAs.

CI Signal Processing



Figure 2. Example signal processing pipeline for CIs.

[1] C.C. Morton, W.E. Nance. (2006) New England Journal of Medicine, 354:2151-64.
[2] F.R. Lin, J.L. Niparko, and L. Ferrucci (2011) Archives of Internal Medicine, 171:1851-3.

CI





Motivation



Limitations in existing research interfaces

- Functionality
 - Lack of bimodal support (electric + acoustic hearing)
- Computation power
 - Must sustain complex signal processing algorithms
- Portability
- Real-time evaluation
- Barrier to entry for unfamiliar programming languages

Not suitable for a broad range of experiments

Proposed attributes

Custom solutions (*i.e.*, direct connection to implants)







CCi-MOBILE



CCi-MOBILE Research Platform

- USB/Wi-Fi research interface configured for both in-laboratory and field testing of sound processing strategies and/or data collection for CI/HA*
- Plug-and-play system (portable, wearable, on-the-go signal processing adjustments)
- Supports time synchronized Fi acoustic and/or electric stimulation
 - Unilateral/bilateral CIs*
 - Bimodal (Electric-Acoustic-Stimulation)
- High-level language software suite (MATLAB, Java)



Figure 3. CCi-MOBILE Research Platform (open-case) in unilateral mode.

Investigational Parameters

- No. electrodes/channels configurations
- Stimulation mode
- Stimulation rate (pps/ch)
- Pulse width (bi-phasic stimulation)
- Proposed signal processing strategies (CISbased**) for unilateral/bilateral

* Supports cochlear implants (CIs) manufactured from Cochlear Ltd. from the CI24 implant series.
 ** Supports signal processing strategies adapted using the Continuous-Interleaved-Strategy (CIS).







- FPGA design programmed in Verilog using Xilinx ISE software
- Real-time performance (minimal processing delay) achieved via buffering of incoming and outgoing data on a frame-by-frame basis
- Variable rate electric stimulation uses 16-bit wide RAM buffers to store information: electrodes and current levels



Figure 5. Hardware implementation & layout orientation of components.

- Parameter matching using inter-pulse-gap, pulsewidth, and inter-phase-gap used to determine accuracy received at the RF-coil
 - Parameters are measured and verified using an externally connected oscilloscope







- Data synchronization managed via RAM and handshake design techniques
- Communication between computing platform and CCi-MOBILE at 5 Mbps
- Sampling of audio data and stereo playback is achieved at 16 kHz
- CI24 implants require a data burst at 5 MHz while the platform operates at 80 MHz



Figure 6. Hardware design architecture for electric and acoustic stimulation (EAS) and variable rate stimulation.



Communication Pipeline



- Hardware/interface-board continuously samples
 incoming analog signals from BTE mic
- 2) Digitizes 512 bytes of audio
- PC/smartphone processes digitized audio into electrical stimuli using signal processing routines
- Generation of electrical signals from electrical stimuli



Figure 7. Processing data communication between CCI-MOBILE & FPGA.

5) Streams data using proprietary communication routines (Cochlear Ltd.) on a frameby-frame basis for CI24 cochlear implant systems

* For bimodal applications, acoustic & electric signals are sent synchronously



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CCi-MOBILE Applications

- Easily record naturalistic audio using build-in audiorecording application(s)
 - Stereo and mono recordings
- Perform lateralization and localization experiments
- Implementation of novel signal processing algorithms for CIs/HAs
 - Speech enhancement, noise suppression, etc.
- Built-in vocoder application to simulate electric-hearing for normal hearing (NH) listeners³

Android App

Real-time performance on Android smartphones and tablets



- Highly suitable for in-field or take-home trials
- Easily adjust signal processing/MAP parameters in real-time
- Quickly select/define pre-programmed environments

Figure 4. Android app for CCi-MOBILE program windows.

[3] H. Ali, N. Mamun, A. Brueggeman, R.C.M.C. Shekar, J.N. Saba, J.H.L. Hansen (**2018**) Conf. Acoust. Soc. Am., 144:1872.



Custom Signal Processing









Custom Signal Processing (SP) Parameter Evaluation

Determine sample loss from customized SP input parameters (stimulation rate, pulse-width, number of electrodes) using a standard 0-150 user-defined MAP

Experimental Set-Up and Results

99.008% of valid configurations resulted in <1% sample loss</p>









Acoustic-Diversity Evaluation

Determine charge (current) from various acoustic input (380 hrs.) of audio, speech, music, noise, etc.

Experimental Set-Up and Results

All charge/current values produced from CCi-MOBILE were within clinical safety limits (safety limit = 350 mC/s)







Clinical-Processor-vs-CCi-MOBILE Evaluation

Compare speech intelligibility of CI users (N=8) using their commercial processors (Cochlear Ltd.) and CCi-MOBILE

Experimental Set-Up and Results

Comparable performance to clinical processors achieved (F[7,49]=4.882, p<0.069)</p>





Conclusions



- CCi-MOBILE is an open-source, flexible research platform compatible with cochlear implants and hearing aids
- Easy-to-use, adaptable applications and templates available for speech scientists in a high-language environment
- Hardware and software verification routines ensure safety and reliability of CCi-MOBILE
- Suited to address multi-disciplinary hearing research topics such as: speech-in-noise, sound localization/lateralization, speech enhancement, custom environmental MAP changes, etc.
- Enables bench-top, in-lab, and field experiments for all speech and hearing scientists



